

**GASTRORETENTIVE DRUG DELIVERY SYSTEM: STOMACH SPECIFIC MUCOADHESIVE TABLET**Siddhapara Mihir\*, Tikare Vijay, Ramana MV, Sutariya Bhavesh, Vaghasiya Bhavesh  
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\*Email: [siddhapara.md@gmail.com](mailto:siddhapara.md@gmail.com)**ABSTRACT**

The current article focuses on the principles of mucoadhesive drug delivery systems based on adhesion to biological surfaces that are covered by mucus. Bioadhesion can be defined as the process by which a natural or a synthetic polymer can adhere to a biological substrate. When the biological substrate is a mucosal layer then the phenomena is known as mucoadhesion. Drug actions can be improved by developing new drug delivery systems, such as the mucoadhesive system. These systems remain in close contact with the absorption tissue, the mucous membrane, releasing the drug at the action site leading to a bioavailability increase and both local and systemic effect. Mucoadhesion is defined as the ability of material adheres to biological tissue for an extended period of time. Mucoadhesive dosage forms extend from the simple oral mucosal delivery to the nasal, vaginal, ocular and rectal drug delivery systems. The success and degree of mucoadhesion bonding is influenced by various polymer-based properties. Evaluation of such mucoadhesive formulations has transgressed from first-generation charged hydrophilic polymer net-works to more specific second generation systems based on lectin, Thiol and various other adhesive functional groups. Various theories are consider like Electronic theory, Wetting theory, Absorption theory, Fracture theory in mucoadhesion. Various *In vitro* and *In vivo* tests carried out for determination of mucoadhesion.

**Keywords:** Mucoadhesion, natural polymer, in-vitro mucoadhesive strength, *In vivo* mucoadhesive strength.

**INTRODUCTION**

Since the last three decade many drug molecules formulated as gastroretentive drug delivery system have been patented keeping in view its commercial success<sup>1</sup>. Oral sustained drug delivery system is complicated by limited gastric residence times (GRTs). Rapid GI transit can prevent complete drug release in the absorption zone and reduce the efficacy of the administered dose since the majority of the drugs are absorbed in stomach or the upper part of small intestine<sup>2, 3</sup>. Therefore, control of placement of a drug delivery system (DDS) in a specific region of the GI tract offers advantages for a variety of important drugs characterized by a narrow absorption window in the GIT or drugs with a stability problem<sup>4</sup>.

These considerations have led to the development of a unique oral controlled release dosage form with gastroretentive properties. After oral administration, such a dosage form would be retained in the stomach and release the drug there in a controlled and prolonged manner, so that the drug could be supplied continuously to its absorption sites in the upper gastrointestinal tract<sup>5</sup>. Gastroretentive dosage form can remain in the gastric region for several hours and hence significantly prolong the gastric residence time of drugs. Prolonged gastric retention improves bioavailability, reduces drug waste, and improves solubility of drugs that are less soluble in a high pH environment. It is also suitable for local drug delivery to the stomach and proximal small intestines<sup>6</sup>.

To overcome these limitations, various approaches have been proposed to increase gastric residence of the drug delivery systems in the upper part of the gastrointestinal tract includes floating drug delivery systems (FDDS)<sup>7,8</sup>, swelling or expanding systems<sup>9</sup>, mucoadhesive systems<sup>10,11</sup>, modified-shape systems<sup>12</sup>, high-density systems<sup>13</sup>, and other delayed gastric emptying devices.

Dosage forms that can be retained in the stomach are called gastroretentive drug delivery system (GRDDS)<sup>14</sup>. These drugs delivery system suffer from mainly two adversities: the short gastric retention time (GRT) and unpredictable short gastric emptying time (GET), which can result in incomplete drug release from the dosage form in the absorption zone leading to diminished efficacy of administered dose<sup>15</sup>.

**Potentially active drug candidates suitable for gastroretention**

The suitable candidates for gastroretentive drug delivery system are molecules that possess poor absorption but are characterized by better absorption<sup>16</sup>:

1. Drugs that have narrow absorption window in gastrointestinal tract.  
E.g. riboflavin and levodopa
2. Drugs that are primarily absorbed from stomach and upper part of gastrointestinal tract.  
E.g. calcium supplements, chlordiazepoxide and cinnarazine
3. Locally active drugs in the stomach.  
E.g. antacids and misoprostol
4. Drugs which degraded or unstable in the colon.  
E.g. ranitidine HCl and metronidazole
5. Drugs that disturb normal colonic bacteria or microbes.  
E.g. amoxicillin trihydrate

**Factor Affecting Gastric Retention**

The most important parameter affecting gastric emptying and gastric retention time of oral dosage form.

1. Density, size and shape of the device<sup>17,18</sup>.
2. Concomitant ingestion of food and its nature, caloric content and frequency of intake<sup>19,20</sup>.
3. Simultaneous administration of drugs with impact on gastrointestinal transit time: drugs acting as anticholinergic agents (e.g. atropine), opiates (e.g. codeine) and prokinetic agents (e.g. metoclopramide, cisapride)<sup>21</sup>.
4. Biological factor such as gender, posture, age, sleep, body mass index, physical activity and disease states (e.g. diabetes, crohn's disease)<sup>22</sup>.

**General Aspects Of Gastrointestinal Tract****Anatomy of the gastrointestinal tract**

The gastrointestinal tract categorized into three main parts:

- a. stomach
- b. Small intestine – Duodenum, jejunum, and ileum
- c. Large intestine

The gastrointestinal tract is a long muscular tube, starting from the mouth and end at the anus, which capture the nutrient inside the body and eliminate by different physiological processes such as secretion, digestion, absorption, excretion. Figure 1 include the basic construction of gastrointestinal tract from stomach to large intestine.

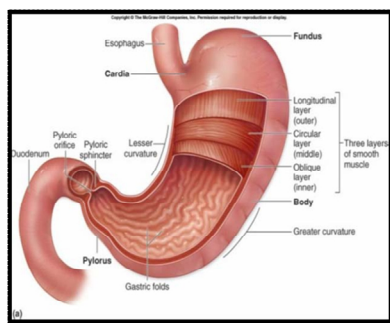


Figure 1: Anatomy of the gastrointestinal tract.

The stomach is a J-shaped organ which can be divided into four parts: cardia, fundus, body and antrum. The main function of the stomach is to store and mix food with gastric secretion.

It consists of serosa, longitudinal muscle, intermuscular plane, circular muscle, submucosa, lamina propria and epithelium. The stomach has a third muscle layer called as the "oblique muscle layer" situated in the proximal stomach, branching over the fundus and higher regions of the gastric body. The different smooth muscle layers are performing the motor function of the gastrointestinal tract, i.e. gastric emptying and intestinal transit<sup>23</sup>.

#### Physiology of the gastrointestinal tract

The proximal part is made up of fundus and body. It serves as a reservoir for the materials which remain undigested, whereas the antrum is the main site for mixing motion and acts as a pump for gastric emptying by propelling actions. Gastric emptying occurs during both fasting as well fed states. During the fasting state an interdigestive series of electrical events takes place, which cycles through stomach and intestine every 2 to 3 hours<sup>24</sup>. This is called the interdigestive myoelectric cycle or migrating myoelectric cycle (MMC), which further divided into following 4 phases as described by Wilson and Washington<sup>25</sup>. (figure 2)

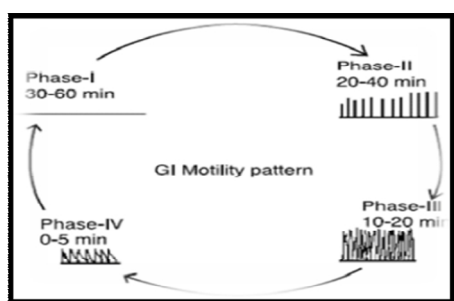


Figure 2: A simplified schematic diagram of the interdigestive balanced motility pattern.

Phase I (basal phase) lasts from 40 to 60 minutes with rate contractions.

Phase II (preburst phase) lasts for 40 to 60 minutes with intermittent action potential and contractions. As the phase progresses the intensity and frequency also increase gradually.

Phase III (burst phase) lasts for 4 to 6 minutes. It includes intense and regular contraction for short period. It is due to this wave that all the undigested material is swept out the stomach down to the small intestine. It is also known as the housekeeper wave.

Phase IV lasts for 0 to 5 minutes and occurs between phases III and I to 2 consecutive cycles.

After the ingestion of a mixed meal, the pattern of contractions changes from fasted to that of fed state. This is also known as digestive motility pattern and comprises continuous contraction as in phase II of fasted state. These contraction result is reducing the size of food particles (to less than 1 mm), which are propelled toward the pylorus in a suspension form. During the fed state onset of MMC is delayed resulting in slowdown of gastric emptying rate<sup>26</sup>.

$\gamma$ -scintigraphy, radiology, endoscopy, ultrasonography, radiotelemetry and magnetic marker monitoring studies have been applied to determining gastric emptying rates revealed that orally administered controlled release dosage forms are subjected to basically 2 complications that of short gastric residence time and unpredictable gastric emptying rate<sup>27,28</sup>.

#### The Mucus Layer

Mucus is a translucent and viscid secretion, which forms a thin, continuous gel blanket adherent to mucosal epithelial surface. The mean thickness of this layer varies from about 50-450  $\mu\text{m}$  in humans. It is secreted by the goblet cells lining the epithelia or by special exocrine glands with mucus cells acini. The exact composition of the mucus layer varies substantially, depending on the species, the anatomical location and pathological states. However, it has general composition<sup>29,30</sup>.

Table no 1: composition of mucus

Sr.no	Composition	% amount
1	Water	95
2	Glycoprotein and lipid	0.5-5.0
3	Minerals salts	1
4	Free proteins	0.5-1.0

#### Function of mucus layer

The primary functions of the mucus layer are<sup>12</sup>

**Protective:** Resulting particularly from its hydrophobic

**Barrier:** The role mucus layer as barrier in tissue absorption of drugs and other substance is well known as it influences the bioavailability of the drugs.

**Adhesion:** Mucus has strong cohesive properties and firmly binds to the epithelial cell surface as continuous layer.

**Lubrication:** an important role of mucus layer is to keep the mucosal membrane moist.

#### Mucoadhesive System

##### Concept

Bioadhesive systems are used as a delivery device within the lumen to enhance drug absorption in a site-specific manner. This approach involves the use of bioadhesive polymers, which can adhere to the epithelial surface in the stomach<sup>31</sup>. The medications that are included in the category of narrow absorption window drugs are mostly associated with improved absorption at the jejunum and ileum due to their enhanced absorption properties, e.g. large surface area, in comparison to the colon or because of the enhanced solubility of the drug in the stomach as opposed to more distal parts of the gastrointestinal tract<sup>32</sup>.

It was suggested that compounding narrow absorption window drugs in a unique pharmaceutical DF with gastro retentive properties would enable an extended absorption phase of these drugs. After oral administration, such a stomach-specific mucoadhesive tablets would be retained in the stomach and release the drug there in a controlled and prolonged manner, so that the drug could be supplied continuously to its absorption sites in the upper gastrointestinal tract. This mode of administration would best achieve the known pharmacokinetic and pharmacodynamic advantages of stomach-specific mucoadhesive tablets for these drugs<sup>33</sup>.

Under certain circumstances prolonging the gastric retention of a delivery system is desirable for achieving greater therapeutic benefit of the drug substance. For example, drugs that are absorbed in the proximal part of the gastrointestinal tract and drugs that are less soluble in or are degraded by the alkaline pH may benefit from prolonged gastric retention. In addition, for local and sustained drug delivery to the stomach and proximal small intestine to treat certain conditions, prolonged gastric retention of the therapeutic moiety may offer numerous advantages including improved bioavailability

and therapeutic efficacy, and possible reduction of dose size. It has been suggested that prolonged local availability of antibacterial agents may augment their effectiveness in treating H. Pylori related peptic ulcers<sup>34,35</sup>.

Various gastrointestinal mucoadhesive dosage forms, such as discs, microspheres, and tablets, have been prepared and reported by several research groups<sup>36</sup>.

#### Adhesion

Adhesion can be defined as the bond produced by contact between a pressure-sensitive adhesive and a surface<sup>38</sup>. The American Society of Testing and Materials has defined it as the state in which two surfaces are held together by interfacial forces which may consist of valence forces, interlocking action, or both<sup>38</sup>.

A bioadhesive is defined as a substance that is capable of interacting with biological materials and being retained on them or holding them together for extended periods of time.

According to Good defined bioadhesion as the state in which two materials, at least one biological in nature, are held together for an extended period of time by interfacial forces. It is also defined as the ability of a material (synthetic or biological) to adhere to a biological tissue for an extended period of time<sup>36</sup>. In biological systems, four types of bioadhesion can be Distinguished<sup>37</sup>.

1. Adhesion of a normal cell on another normal cell
2. Adhesion of a cell with a foreign substance
3. Adhesion of a normal cell to a pathological cell
4. Adhesion of an adhesive to a biological substrate

Bioadhesive are classified into three types based on phenomenological observation, rather than on the mechanisms of bioadhesion.

**Type I:** Bioadhesion is characterized by adhesion occurring between biological objects without involvement of artificial materials. Cell fusion and cell aggregation are good examples.

**Type II:** Bioadhesion can be represented by cell adhesion onto culture dishes or adhesion to a variety of substances including metals, woods, and other synthetic materials.

**Type III:** Bioadhesion can be described as adhesion of artificial substances to biological Substrates such as adhesion of polymers to skin or other soft tissues<sup>35</sup>.

#### Theory Of Mucoadhesions

Several bioadhesion theories have been discussed<sup>40</sup>.

#### Electronic theory

It defined as the electron transfer from contact of an adhesive polymer with a glycoprotein network; they form an electrical interface at adhesive polymer and glycoprotein network. Adhesion can produce by attractive forces across the double layer.

#### Absorption theory

Absorption theory are defined as they cause after initial contact between two surfaces that is material surface because a force formed between two surfaces, the force is two types of chemical bond that is,

1. Primary chemical bond of covalent bond: they are high strength so they cause permanent bonds.
2. Secondary chemical bond has types of force of attraction like electrostatic force, Vander Waals forces, hydrogen and hydrophobic bonds.

#### Wetting theory

They are only beneficial for liquid bioadhesive systems, analyses adhesive and contact behaviour means they have ability of a liquid or a paste to spread over a biological system.

The equation is  $W_a = Y_a + Y_b - Y_{ab}$

Here,  $W_a$  = work of adhesion = energy/cm<sup>2</sup>

a and b= biological membrane

Work of cohesion equation is  $W_c = 2Y_A - (Y_A + Y_{AB})$

$W_c = 2Y_{A \text{ or } B}$

Bioadhesive material B spreading on a biological substrate A so spreading coefficient that is,

$SB/A = Y_A - (Y_B + Y_{AB})$

SB/A should be positive for a bioadhesive material to adhere to a biological membrane.

#### Diffusion Theory

This theory provides the information the polymer chains and the mucus mix to a sufficient depth to form a semi permanent adhesive bond. The polymer chains penetrate the mucus depends on the diffusion coefficient and the time of contact.

#### Fracture Theory

This theory related for difficulty of separation of two surfaces after adhesion,

The equation,  $G = (E e/L)^{1/2}$

E = Young's formula of elasticity

e = Fracture energy

L= Critical crack length

#### Mucoadhesive Polymers<sup>29</sup>

Various mucoadhesive polymers are used in gastroretentive Mucoadhesive drug delivery system. There are two classes of mucoadhesive polymer 1) hydrophilic polymer 2) hydrogels

In the large classes of hydrophilic polymers containing carboxylic group<sup>40, 41</sup> those exhibit best mucoadhesive properties. Poly vinyl pyrrolidone (PVP), Methyl cellulose (MC), Sodium carboxy methyl cellulose (SCMC), hydroxy propyl cellulose (HPC) and other cellulose derivative.

Hydrogels those are exhibit the basic characteristics of an hydrogels to swell by absorbing water interacting by means of adhesion with the mucus that covers epithelia.

- Anionic group - Carbopol<sup>42</sup>, Polyacrylates and their crosslinked modifications.
- Cationic groups - Chitosan and its derivatives.
- Neutral groups - Eudragit-NE30D etc.

Table 2: some mucoadhesive polymers<sup>43</sup>

Natural	Synthetic	Biocompatible	Biodegradable
Na alginate	Polyvinyl alcohol, Polyamides, polycarbonates, Polyalkylene glycols, Polyvinyl esters.	Esters of haluronic acid.	Poly (lactides)
Pectin		Polyvinyl acetate	Poly(glycolides)
Tragacanth	Esters and halides, Polymethacrylic acid, Polymethyl methacrylic acid.	Ethylene glycol	Poly (lactides-co-glycolides), Polycaprolactones.
Gelatin			
Carrageenan	Methylcellulose, Ethylcellulose, Hydroxy - propyl cellulose, Hydroxy propyl methyl -cellulose.		Polyalkyl cynoacrylates, Polyorthoesters, Polyphosphoesters, Polyanhydrides.
Gum karaya	Sodium carboxymethylcellulose		Polyphosphazenes
Gum ghatti			Chitosan
			Polyethylene oxide

### Characteristics of mucoadhesive polymer

1. The polymer and its degradation products should be nontoxic and should be no absorbable from the GI tract.
2. It should be non-irritant to the mucus membrane.
3. It should preferably form a strong no covalent bond with the mucin-epithelial cell surfaces.
4. It should adhere quickly to most tissue and should possess some site specificity.
5. It should allow easy incorporation of the drug and should offer no hindrance to its release.
6. The polymers must not decompose on storage or during the shelf life of the dosage form.
7. The cost of polymer should not be high so that the prepared dosage form remains competitive.

Robinson and his group using the fluorescence technique, concluded that:

1. Cationic and anionic polymers bind more effectively than neutral polymers.
2. Polyanions are better than polycations in terms of binding/potential toxicity, and further, that water-insoluble polymers give greater flexibility in dosage form design compared with rapidly or slowly dissolving watersoluble polymers.
3. Anionic polymers with sulfate groups bind more effectively than those with carboxylic groups.
4. Degree of binding is proportional to the charge density on the polymer.
5. Highly binding polymers include carboxy methyl cellulose, gelatine, hyaluronic acid, carbopol, and polycarbophyl<sup>44</sup>.

### Factors Affecting Mucoadhesion

These are the factors which are affecting on mucoadhesion given as below<sup>29, 42</sup>.

#### 1. Polymer related factors

- a. Molecular weight
- b. Concentration of active polymer
- c. Flexibility of polymer chains
- d. Special confirmation
- e. Swelling

#### 2. Environment related factors

- a. pH of polymer - substrate interface
- b. Applied strength
- c. Initial contact time

#### 3. Physiological factors

- a. Mucin turns over
- b. Disease state

### 1. Polymer-Related Factors

#### Molecular weight

The optimum molecular weight for maximum bioadhesion depends upon type of mucoadhesive polymer at issue. It is generally understood that the threshold required for successful bioadhesion is at least 100 000 molecular weight. For example, polyethylene glycol (PEG), with a molecular weight of 20 000, has little adhesive character, whereas PEG with 200 000 molecular weight has improved, and PEG with 400 000 has superior adhesive properties. The fact that mucoadhesiveness improves with increasing molecular weight for linear polymers implies two things: (1) interpenetration is more critical for a low-molecular-weight polymer to be a good mucoadhesive, and (2) entanglement is important for high-molecular-weight polymers.

#### Concentration of active polymer

There is an optimum concentration for a mucoadhesive polymer to produce maximum bioadhesion. In highly concentrated system, beyond the optimum level, however, the adhesive strength drops significantly because the coiled molecules become separated from the medium so that the chain available for interpenetration becomes limited.

#### Flexibility of polymer chains

Chain flexibility is critical for interpenetration and entanglement. As water soluble polymers become crosslinked, the mobility of an individual polymer chain decreases and thus the effective length of the chain that can penetrate into the mucus layer decreases, which reduces mucoadhesive strength.

#### Spatial conformation

Besides molecular weight or chain length, spatial conformation of a molecule is also important. Despite a high molecular weight of 19 500 000 for dextrans, they have adhesive strength similar to that of PEG, with a molecular weight of 200 000. The helical conformation of dextran may shield many adhesively active groups, primarily responsible for adhesion, unlike PEG polymers, which have a linear conformation.

#### Swelling

Swelling characteristics are related to the mucoadhesive itself and its environment. Swelling depends on the polymer concentration, the ionic strength, and the presence of water. During the dynamic process of bioadhesion, maximum bioadhesion in vitro occurs with optimum water content. Over hydration will results in the formation of wet slippery mucilage without adhesion.

### 2. Environment-Related Factors

#### pH of polymer-substrate interface

pH can influence the formal charge on the surface of the mucus as well as certain ionizable mucoadhesive polymers. Mucus will have a different charge density depending on pH due to the difference in



dissociation of functional groups on the carbohydrate moiety and the amino acids of the polypeptide backbone. Some studies had shown that the pH of the medium is important for the degree of hydration of cross-linked polycyclic acid, showing consistently increased hydration from pH 4 through pH 7, and then a decrease as alkalinity or ionic strength increases, for example polycarboxylic acid does not show a strong mucoadhesive property above pH 5 because uncharged, rather than ionized, carboxyl group reacts with mucin molecule, presumably through numerous hydrogen bonds. However, at higher pH, the chain is fully extended due to electrostatic repulsion of the carboxylate anions.

#### Applied strength

To place a solid mucoadhesive system, it is necessary to apply a defined strength. Whatever the polymer, poly (acrylic acid/divinyl benzene) or carbopol 934, the adhesion strength increases with the applied strength or with the duration of its application, up to an optimum. The pressure initially applied to the mucoadhesive tissue contact site can affect the depth of interpenetration. If high pressure is applied for a sufficiently long period of time, polymers become mucoadhesive even though they do not have attractive interactions with mucin.

#### Initial contact time

Contact time between the mucoadhesive and mucus layer determines the extent of swelling and interpenetration of the mucoadhesive polymer chains. More mucoadhesive strength increases as the initial contact time increases.

### 3. Physiological Factors

#### Mucin turnover

The natural turnover of mucin molecules from the mucus layer is important for at least two reasons. Firstly, the mucin turnover is expected to limit the residence time of the mucoadhesives on the mucus layer. No matter how high the mucoadhesive strength, they are detached from the surface due to mucin turnover. The turnover rate may be different in the presence of mucoadhesives, but no information is available on this aspect. Secondly, mucin turnover results in substantial amounts of soluble mucin molecules. These molecules interact with mucoadhesives before they have chance to interact with the mucus layer. Surface fouling is unfavourable for mucoadhesion to the tissue surface. Mucin turnover may depend on the other factors such as the presence of food. The gastric mucosa accumulates secreted mucin on the luminal surface of the tissue during the early stages of fasting. The accumulated mucin is subsequently released by freshly secreted acid or simply by the passage of ingested food; the exact turnover rate of the mucus layer remains to be determined.

#### Disease state

The physicochemical properties of the mucus are known to change during disease conditions such as the common cold, gastric ulcers, ulcerative colitis, cystic fibrosis, bacterial, and fungal infections of female reproductive tract, and inflammatory conditions of the eye. The exact structural changes taking place in mucus under these conditions are not clearly understood. If mucoadhesives are to be used in the disease states, the mucoadhesive property needs to be evaluated under the same conditions.

#### Evaluation Of Mucoadhesive Tablets

Various evaluation parameter were carried out for mucoadhesive tablets<sup>43, 29</sup>.

#### General Appearance

The general appearance of a tablet, its visual identity and overall "elegance" is essential for consumer acceptance for control of lot-to-lot uniformity and general tablet-to-tablet uniformity and for monitoring trouble free manufacturing.

The control of the general appearance of a tablet involves the measurement of a number of attributes such as a tablet's size, shape,

color, presence or absence of an odor, taste, surface texture, physical flaws and consistency<sup>43</sup>.

#### Hardness

Hardness was measured by Monsanto hardness tester and Pfizer tester were used<sup>44,45</sup>.

#### Friability

Twenty tablets were weighed and placed in the Roche friabilator and apparatus was rotated at 25 rpm for 4 minutes. After revolutions the tablets were dusted and weighed again. The percentage friability was measured using the formula<sup>43,45</sup>,

$$\% F = \{1 - (W_o/W)\} \times 100$$

Where, % F = friability in percentage

W<sub>o</sub> = Initial weight of tablet

W = weight of tablets after revolution

#### Weight variation

Twenty tablets were randomly selected from each batch and individually weighed. The average weight and standard deviation of 20 tablets was calculated. The batch passes the test for weight variation test if not more than two of the individual tablet weight deviates from the average weight by more than the percentage shown in Table No.3 and none deviate by more than twice the percentage shown<sup>43, 46</sup>.

Table 3: percentage deviation allowed under weight variation test

Average weight of tablets	Percentage deviation
130 or less	10
130-324	7.5
More than 324	5

#### Swelling index

Swelling of tablet excipients particles involves the absorption of a liquid resulting in an increase in weight and volume. Liquid uptake by the particle may be due to saturation of capillary spaces within the particles or hydration of macromolecule. The liquid enters the particles through pores and bind to large molecule, breaking the hydrogen bond and resulting in the swelling of particle. The extent of swelling can be measured in terms of % weight gain by the tablet<sup>47, 48, 49</sup>.

#### Method

For each formulation batch, one tablet was weighed and placed in a beaker containing 200 ml of buffer media. After each interval the tablet was removed from beaker and weighed again up to 8 hours. The swelling index was calculated using following formula.

$$\text{Swelling Index (S.I.)} = (W_t - W_o) / W_o$$

Where, S.I. = Swelling index

W<sub>t</sub> = Weight of tablet at time t

W<sub>o</sub> = Weight of tablet before placing in the beaker.

#### In vitro release study

Standard USP or IP dissolution apparatus have been used to study in vitro release profile using both basket and rotating paddle. In vitro release rate study of mucoadhesive tablet of was carried out using the Apparatus 2 (Basket apparatus) method. Place the tablet in a dry basket at the beginning of each test. Lower the Basket before rotation operates the apparatus immediately at 50 rpm. Medium used for release rate study was 900ml 0.1 N HCl during the course of study whole assembly was maintained at 37±0.5 °C. Withdraw a 5 ml of sample at specific time interval and replaced with 5 ml of fresh dissolution medium. The withdrawn samples were dilute with dissolution medium and then filter it with whattman filter paper and assayed. The % release of drug was calculated<sup>29, 50</sup>.

## *In vitro* Mucoadhesive strength

### 1) Shear stress method

Two smooth, polished plexi glass blocks were selected; one glass block was fixed with an adhesive on the other glass block which was fixed on to the levelled table. To the upper block a thread was tied and the thread was passed down through a pulley. At the end of the thread a beaker was fixed. The length of the thread from pulley to the beaker was 7 cms. The weight of the beaker was counteracted. The assembly is shown in the figure 3. Solutions of different gums, combination of gums and synthetic polymer were prepared. A fixed volume (0.5ml) of solution of natural gums, their combination and Carbopol 934 P were kept on the centre of the fixed glass block with the help of the pipette, and the second block was placed on the first block and pressed by applying 100 g of weight, so that the drop of synthetic polymer, natural gums and the combination of the gum solutions spreads as a uniform film in between the two blocks. After keeping it for a fixed time intervals of 5, 10, 20 and 30 min, purified water was added into the beaker gradually, the weight of purified water just sufficient to pull the upper block or to make it slide down from the base block was recorded. This weight was considered as the adhesive strength i.e. shear stress required to measure the adhesion. Before every experiment care was taken so that no air is entrapped in between the two blocks which might give erratic results. The distance from pulley to the glass block was always same in the observations<sup>51</sup>.

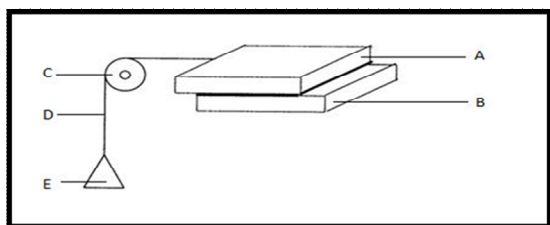


Figure 3:(The assembly used in the shear stress measurement method)  
(A)Upper glass plate (B) Lower glass plate (C) Pulley (D) Thread (E) Pan

### 2) Wilhelmy plate method

In this method small glass plates were coated uniformly by solution of gums, their combination and synthetic polymer to be tested and dried at 60°C. The prepared coated plates were immersed in buffer solution (pH 1.2), for 5, 10, 20, and 30 min at room temperature. The force required to pull the plate out of the solution was determined under constant experimental conditions<sup>51</sup>.

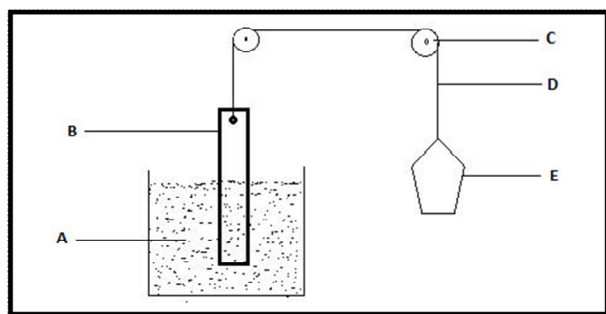


Figure 4: *In vitro* mucoadhesive strength measurement apparatus  
(A)Gastric fluid (pH 1.2) (B) Coated glass plate (C) Pulley (D) Thread (E) Pan

### 3) Modified physical balance method

The mucoadhesive strength of the tablets was measured on an modified physical balance. The apparatus consist of a modified double beam physical balance in which the right and left pan were with lighter pans. The left side of the balance was made heavier than the right side by placing a 5 g weight on left side pan. Another Teflon block of 3.8 cm diameter and 2 cm height was fabricated

with an upward protrusion of 2 cm height and 1.5 cm diameter on one side. This was kept in the beaker, which was then placed below the left hand set of the balance. The goat gastric mucus membrane was used as the model membrane and pH 1.2 buffer solution was used as the moistening fluid. The goat stomach mucosa was kept in tyrode solution at 37°C for 2 hr. The underlying mucus membrane was separated and washed thoroughly with a pH 1.2 buffer solution. It was then tied to a Teflon-coated glass slide and this slide was fixed over the protrusion in the Teflon block using a thread. The block was then kept in a beaker containing pH 1.2 buffer solution at a level that just touches the membrane so as to moisten the membrane. By keeping a 5 g weight on the right pan that two sides were balanced. The beaker with the Teflon block was kept below the left hand setup of the balance. The tablet was stuck on to the lower side of the left hand side pan. The 5 g weight from the right pan was then removed. This lowered the left pan along with the tablet over the membrane with the weight of 5 g. This was kept undisturbed for 3 min. Then the weight on the right hand side was added in an increment of 0.5 g until the tablet just separates from the membrane surface. The excess weight on the right pan i.e. total weight minus 5 g was taken as the measure of the mucoadhesive strength from the mucoadhesive strength, the force of adhesion was calculated using following formula<sup>52,53,54</sup>.

$$\text{Force of adhesion (N)} = \text{Mucoadhesive strength}/100 \times 9.81$$

## *In vivo* techniques

### 1. GI Transit using Radio-Opaque Tablets

It is a simple procedure involving the use of radio-opaque markers, e.g. barium sulfate, encapsulated in mucoadhesive tablets to determine the effects of mucoadhesive polymers on GI transit time. Feces collection (using an automated feces collection machine) and X-ray inspection provide a non-invasive method of monitoring total GI residence time without affecting normal GI motility. Mucoadhesives labelled with Cr-51, Tc- 99m, In-113m, or I-123 have been used to study the transit of the tablets in the GI tract<sup>49</sup>.

### 2. Gamma Scintigraphy Technique

Distribution and retention time of the mucoadhesive tablets can be studied using the gamma scintigraphy technique. A study has reported the intensity and distribution of radioactivity in the genital tract after administration of technetium-labelled HYAFF tablets. Dimensions of the stomach part of the sheep can be outlined and imaged using labelled gellan gum, and the data collected are subsequently used to compare the distribution of radiolabeled HYAFF formulations. The retention of mucoadhesive-radiolabeled tablets based on HYAFF polymer was found to be more for the dry powder formulation than for the pessary formulation after 12 h of administration to stomach epithelium. The combination of the sheep model and the gamma scintigraphy method has been proved to be an extremely useful tool for evaluating the distribution, spreading, and clearance of administered stomach mucoadhesive tablets<sup>49</sup>.

### Stability study

Stability studies were performed according to ICH guidelines. The formulations were stored in room temperature at  $25 \pm 1^\circ$ , in hot air oven at  $37 \pm 1^\circ$ , and at  $60 \pm 1^\circ$  for a period of 14 weeks<sup>55</sup>.

## CONCLUSION

Mucoadhesive dosage forms have a high potential of being useful means of delivering drugs to the body, perhaps particularly for topical or local administration where the mechanical trauma experienced by the dosage form may be minimized. The phenomenon of mucoadhesion can be used as a model for the controlled drug delivery approaches for a number of drug candidates. The various advantages of the oral mucoadhesive drug delivery systems like prolongation of the residence time of the drug which in turn increases the absorption of the drug are important factors in the oral bioavailability of many drugs.

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